Cost-effective elimination of lipofuscin fluorescence from formalin-fixed brain tissue by white phosphor light emitting diode array

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1 Cost-effective elimination of lipofuscin fluorescence from formalin-fixed brain tissue by
2 white phosphor light emitting diode array

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11 **ABSTRACT:**

12 Autofluorescence of aldehyde-fixed tissues greatly hinders fluorescence microscopy. In
 13 particular, lipofuscin, an autofluorescent component of aged brain tissue, complicates
 14 fluorescence imaging of tissue in neurodegenerative diseases. Background and lipofuscin
 15 fluorescence can be reduced by greater than 90% through photobleaching using white phosphor
 16 light emitting diode arrays prior to treatment with fluorescent probes. We compared the effect of
 17 photobleaching versus established chemical quenchers on the quality of fluorescent staining in
 18 formalin-fixed brain tissue of frontotemporal dementia with tau-positive inclusions. Unlike
 19 chemical quenchers, which reduced fluorescent probe signals as well as background,
 20 photobleaching treatment had no effect on probe fluorescence intensity while it effectively
 21 reduced background and lipofuscin fluorescence. The advantages and versatility of
 22 photobleaching over established methods are discussed.

23 Keywords: autofluorescence; lipofuscin; photobleaching; light emitting diode; fluorescence
 24 microscopy

25 INTRODUCTION:

26 The successful visualization of fluorescent markers in tissue is often complicated by
27 autofluorescence. Many sources of endogenous autofluorescence exist in mammalian tissues,
28 such as lipofuscin, collagen, and elastin (Banerjee et al. 1999, Ottis et al. 2012). Formalin
29 fixation, a common method of sample preparation, also generates autofluorescence. Lipofuscin,
30 whose presence is a common hallmark of aging, is a particular complication in fluorescence
31 imaging of specimens of neurodegenerative diseases, where patients are often of advanced age
32 (Ottis et al. 2012). Lipofuscin's broad fluorescence emission greatly hinders the application of
33 common fluorescent labels like FITC and Texas Red. Lipofuscin signals often need to be
34 manually labeled in fluorescence images to aid image interpretation (Xiao et al. 2015).

35 A number of treatment options have been suggested to reduce lipofuscin fluorescence. These
36 include chemical treatment of the specimen with CuSO_4 in ammonium acetate or quenching dyes
37 such as Sudan Black B and Eriochrome Black T (Davis et al. 2014). Digital image processing by
38 spectral un-mixing has also been used, but the process is difficult and has the disadvantage of
39 generating false positives and artifacts (Zimmermann et al. 2003). Previously, photobleaching
40 using a fluorescent tube lamp has been performed, although certain lipofuscin structures still
41 remain unaffected after 48 hours in brain tumour sections (Neumann and Gabel 2002). It has also
42 been reported previously that RGB-based, multispectral light emitting diode (LED) arrays are
43 effective at reducing autofluorescence, though the apparatus may be cost-prohibitive (Duong and
44 Han 2013). The most thorough photobleaching can be achieved by irradiating the sample under a
45 fluorescence microscope using a high powered laser source through an objective (Schnell et al.
46 1999, Neumann and Gabel 2002). However, this method is impractical due to the limited field of

view of the objective compared to the size of the sample. Prolonged exposure will also cause sample damage.

Recently, white phosphor LEDs used in household lighting have emerged as an alternative light source for fluorescence microscopy over halogen lamps due to their wide emission spectrum, high luminosity, and very low manufacturing cost (Albeanu et al. 2008, Robertson et al. 2009). Phosphor-based LEDs generate white light through a single blue LED surrounded by yellow phosphors, and are less costly than their RGB-based counterparts. Given the viability of white LEDs as a fluorescence excitation source, we propose a simple, effective, and widely applicable method to reduce autofluorescence from formalin-fixed tissue by photobleaching the specimen using a commercially available LED lamp prior to staining and immunofluorescence imaging. In the study by Duong and Han, an apparatus was constructed using custom scaffolds, slide holders, and an array of high power multispectral LEDs in an enclosed refrigeration unit. The cost of raw materials, fabrication and construction for this apparatus may be upwards of 1000 USD. In the present study, we show that an equivalent result can be achieved using off-the-shelf components for less than 1% of the cost.

We quantified the efficacy of white phosphor LED photobleaching in formalin-fixed human brain tissue from a patient with frontotemporal lobar degeneration with tau-positive inclusions (FTLD-T). We stained the tissue with a number of fluorescent probes and compared and quantified the quality of staining in sections that have been pre-treated with photobleaching or treated with chemical quenchers TrueBlack™ (a proprietary formula) or Eriochrome Black T. We demonstrate that photobleaching, unlike chemical quenchers, does not suppress fluorescent probe signals.

69 MATERIALS AND METHODS:

70 *Photobleaching apparatus*

71 A 6 watt, 800 lux LED array desk lamp with flexible arm and flat lighting surface (DBpower,
72 Shenzhen, Guangdong, China) was inverted such that the lamp could be placed under a square
73 petri dish (Sarstedt, Nümbrecht, Germany) containing sterile buffer. The dish was elevated by a
74 plastic support to avoid sample heating (Figure 1A). Samples on microscope slides were
75 photobleached by submerging the slides in sterile TBS and 0.05% sodium azide at 4 °C in a cold
76 room. A reflective dome covered the petri dish containing the sample for the duration of
77 photobleaching. The emission spectrum (400-800 nm) of the lamp was measured using a QM-1
78 fluorescence spectrophotometer (Photon Technology International, Edison, NJ, USA).

79 *Sample preparation and Immunofluorescence*

80 Formalin-fixed brain blocks of the orbitofrontal gyri in a case of FTLD-T (~2 days fixation)
81 were run through 10%, 20%, and 30% sucrose gradients, infiltrated with optimal cutting
82 temperature (OCT) compound, frozen, and cut into 10 µm thick sections and attached to glass
83 microscope slides. For samples undergoing photobleaching treatment, slides were photobleached
84 for 48 hours in the photobleaching apparatus prior to staining. The slides were treated in antigen
85 retrieval buffer (10 mM Citric Acid, 2 mM EDTA, 0.05% Tween 20, pH 6.2) for 30 minutes at
86 90 °C, then washed twice for 5 minutes in TBS plus 0.025% Triton X-100 (TBS-Triton). The
87 slides were blocked in 10% normal goat serum (Aurion, Wageningen, The Netherlands) and 1%
88 BSA (ThermoFisher Scientific, Waltham, MA, USA) in TBS-Triton for 2 hours at room
89 temperature. Primary mouse anti-phospho-PHF-tau pSer202+Thr205 (AT8) antibody (1:50,
90 ThermoFisher Scientific, Waltham, MA, USA) in 1% BSA/TBS was applied overnight at 4 °C in

a humidified chamber. The slides were rinsed 2×5 min with TBS-Triton and a mix of secondary antibodies consisting of Alexa 488 goat anti-mouse (1:100, ThermoFisher Scientific, Waltham, MA, USA) and Texas red goat anti-mouse (1:100, ThermoFisher Scientific, Waltham, MA, USA) in 1% BSA/TBS was applied for 1 hour at room temperature in the dark. The slides were rinsed 2×5 min in TBS and stained with DAPI (0.25 $\mu\text{g/mL}$, ThermoFisher Scientific, Waltham, MA, USA) for 10 minutes. Slides not receiving photobleaching treatment were then either treated with TrueBlack™ lipofuscin autofluorescence quencher (Biotium, Hayward, CA, USA) according to manufacturer's instructions or with 1.65% Eriochrome Black T (Sigma-Aldrich, St. Louis, MO, USA) in ddH₂O for 5 minutes according to established protocols (Davis et al. 2014). The slides were rinsed 3×5 min in TBS to remove excess quencher and mounted with Immu-mount aqueous mounting medium (ThermoFisher Scientific, Waltham, MA, USA) for fluorescence microscopy. For Nissl staining, the above protocol was altered such that the blocking and antibody diluting buffers contained 0.5% fish gelatin (Electron Microscopy Sciences, Hatfield, PA, USA) in TBS instead of BSA or serum, and only Alexa 488 conjugated antibody was used for secondary antibody staining. Following DAPI staining and prior to mounting, NeuroTrace® 530/615 red fluorescent Nissl stain (ThermoFisher Scientific, Waltham, MA, USA) was applied to the slides according to manufacturer's instructions.

Fluorescence microscopy and image quantitation

For detection of autofluorescence, several unstained sections were photobleached using the photobleaching apparatus for up to 72 hours. At various time points, the slides were removed from the photobleaching apparatus, coverslipped in sterile TBS and imaged using a Zeiss LSM 710 confocal microscope (Zeiss, Oberkochen, Germany) with a Plan Apochromat 10 $\times$ 0.45 NA objective (Zeiss, Oberkochen, Germany). For the Alexa 488 channel, the sample was excited at

114 488 nm (argon laser) and detected at 493-570 nm. For the Texas Red channel, the sample was
115 excited at 561 nm (DPSS 561 nm laser) and detected at 601-635 nm. For stained slides,
116 fluorescence at Alexa 488 ($\lambda_{\text{ex}} = 488$ nm, $\lambda_{\text{em}} = 493$ -605 nm), Texas Red/Nissl ($\lambda_{\text{ex}} = 561$ nm, λ_{em}
117 $= 566$ -689 nm), and DAPI ($\lambda_{\text{ex}} = 405$ nm; Diode 405 laser, $\lambda_{\text{em}} = 410$ –507 nm) channels were
118 measured. Laser power and gain settings were kept identical using Zen software for each set of
119 comparative images. Lipofuscin fluorescence was quantified by particle analysis in ImageJ
120 (Schneider et al. 2012), plotted, and fitted to a single exponential decay function $y = y_0 + Ae^{\frac{-x}{T}}$
121 using Origin 8.5 software (OriginLab, Northampton, MA, USA), where y is the intensity, x is the
122 photobleaching duration and T is the decay constant. Fluorescence RGB profiling was measured
123 using ImageJ and the 'RGBProfiler' ImageJ plugin ([http://rsb.info.nih.gov/ij/plugins/rgb-](http://rsb.info.nih.gov/ij/plugins/rgb-profiler.html)
124 [profiler.html](http://rsb.info.nih.gov/ij/plugins/rgb-profiler.html)).

RESULTS AND DISCUSSION:

Photobleaching significantly reduces autofluorescence

Autofluorescence of unstained brain tissue from a case of FLTD-T was measured before photobleaching and at 12 hour intervals of LED photobleaching. The emission peaks of the lamp at 450 nm and 500-600 nm suggests that it can effectively target the excitation wavelengths of a broad range of visible-light chromophores (Figure 1B). While previous studies targeted individual emission peaks with multispectral LEDs (Duong and Han 2013), we found that white phosphor LEDs could produce a similar emission spectrum. It was evident from the photographs of the sections that the majority of background fluorescence was eliminated after 24 hours (Figure 1C), while the fluorescent, lipofuscin-like speckles were nearly all photobleached after 72 hours. Using the exponential decay function for quantification, we calculated the half-life of fluorescent intensity to be 4.6 and 7.1 hours for Alexa 488 and Texas Red channels respectively (Figure 2), however, particles with reduced intensities were still generally visible in the photographs at this stage (Figure 1C). Using the decay constants, we calculated that 95% of the fluorescence should be removed after 20 and 31 hours for the Alexa 488 and Texas Red channels respectively. Visually, we found that after 36 hour photobleaching, the intensities of lipofuscin particles became sufficiently low compared to intended fluorescent signals, allowing for generation of immunofluorescence images with little to no background. We used 48 hours as a convenient and effective photobleaching duration for subsequent experiments.

Immunostaining of tau-positive inclusions

Immunostaining for hyperphosphorylated tau was performed to visualize pathological tau inclusions in the FTLTD-T case (Figure 3). We tested the efficacy of 48 hour photobleaching (PB)

147 compared to a commercially available lipofuscin autofluorescence quencher TrueBlack™ (TB)
148 and a previously reported treatment protocol using Eriochrome Black T (EBT) (Davis et al.
149 2014). The tissues were stained with AT8 antibody, followed by commonly used Alexa 488- and
150 Texas Red-conjugated fluorescent secondary antibodies and counterstained with the nuclear stain
151 DAPI. In the untreated sample, autofluorescence was ubiquitous in both the Texas Red and
152 Alexa 488 channels, significantly compromising the quality of the image. Signal profiling of the
153 image showed that the tau inclusions were stained with relatively high intensity for both
154 secondary antibodies. However, the lipofuscin intensity in the Texas Red channel was
155 comparable to the intensity of the Texas Red secondary fluorescence, leading to complications in
156 image interpretation. EBT-treated samples showed over-quenching and complete loss of the
157 DAPI signal. The dye also generated an undesirable basal level of fluorescence in the Texas Red
158 channel. EBT appeared to be effective in reducing Alexa 488 channel autofluorescence, but
159 indiscriminately reduced the secondary antibody fluorescence as well, limiting its utility. Both 48
160 hour PB and TB treatment produced images with minimal background fluorescence. However, in
161 the 48 hour PB treatment, intensities of tau inclusions labeled by Alexa 488 and Texas Red
162 fluorescence were relatively similar based on their signal profiles, whereas the samples treated
163 with TB had significantly reduced Texas Red and DAPI signals.

164 We then investigated the effect of PB and TB treatments on more sensitive stains such as Nissl,
165 which can be quenched by BSA and other serum proteins (Figure 4). We stained the tissue with
166 AT8 primary antibody followed by Alexa 488 secondary as before and applied NeuroTrace®
167 515/630 Nissl stain which labeled neurons within the tissue. The specimen was counterstained
168 with DAPI. Similar to our previous results, PB treatment did not appear to weaken the
169 fluorescence of the Nissl stain in the 570-690 nm emission range, and the cell bodies of the

neurons were readily visible and distinct from the DAPI nuclear staining. In contrast, the TB treated samples showed reduced Nissl staining which largely overlapped with the DAPI signal (Figure 4). It is possible that the TB treatment quenched the weaker staining of Nissl bodies in the endoplasmic reticulum, but did not penetrate into the nucleus, which Nissl also stains (Kádár et al. 2009).

Overall, we find that irradiation of formalin-fixed brain tissue with a white phosphor LED lamp is an effective and low-cost method of reducing autofluorescence. Photobleaching does not interfere with the fluorescence intensity of probes due to the fact that it can be applied prior to sample staining. This allows for exclusive bleaching of unwanted autofluorescence, whereas commercial dyes and quenchers such as TrueBlack™ are applied prior to mounting the sample, allowing for undesirable quenching of probe signals. Additionally, photobleaching does not introduce any exogenous material to the specimen that potentially interferes with subsequent handling. Quenchers such as TrueBlack™ must also be applied in 70% ethanol. Compared to the commercial quencher TrueBlack™, our photobleaching protocol, which uses a commercial lamp, requires more processing time. Our LED array is also not expected to photobleach fluorescence excitable near UV range since the lamp has no emission at wavelengths below 405 nm.

However, LED with higher power and intensity can reduce the processing time, and as previous studies have described, custom LEDs with different emission wavelengths can be used to direct photobleaching to specific chromophores (Duong and Han 2013). For targeting broad-spectrum autofluorescence, however, it appears that white phosphor LEDs is sufficiently effective.

We demonstrate that photobleaching treatment followed by immunostaining generally produces signals that are brighter and more intense at certain wavelengths compared to post-staining autofluorescence suppression approaches, while producing little to no background. The

generation of clean images for immunofluorescence microscopy is not only important for the accurate visualization of features of interest, but it is also a prerequisite for the application of advanced microscopy techniques such as spatially targeted optical micro-proteomics (STOMP) (Hadley et al. 2015). While previous methods have involved intricately assemblies, we present an extremely simple, inexpensive, but effective method for autofluorescence removal that is accessible to all investigators. Overall, photobleaching using white phosphor LED prior to staining is a versatile treatment that we expect to be amiable to a broad range of specimens.

AUTHOR CONTRIBUTIONS:

Y. S contributed to experimental design, conducted experiments, and analyzed data. A. C. conceived the study. All authors participated in the drafting of the manuscript.

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ETHICS:

The work presented was performed in compliance with recognized international standards, including the International Conference on Harmonization (ICH), the Council for International Organizations of Medical Sciences (CIOMS) and the principles of the Declaration of Helsinki. Use of human tissue was in accordance with the University Health Network Research Ethic

215 Board. The human brain samples were collected as a part of the Maritime Brain Tissue Bank. At
216 the time of collection, informed consent was obtained.

217 **COMPETING INTERESTS:**

218 The authors declare no competing interests.

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253 **FIGURE LEGENDS:**

254 **Figure 1: Time-dependent photobleaching of formalin-fixed brain tissue using a white**
255 **phosphor LED array.** A) Photograph of photobleaching apparatus indicating the LED array
256 light source, plastic platform, and sample chamber where a mock slide is placed in buffer. A
257 reflective dome is constructed using aluminum foil to cover the apparatus during photobleaching.
258 B) Emission spectrum of LED array consists of a sharp peak at 450 nm and a broad peak
259 centered at 550 nm and spanning 500-600 nm (arbitrary fluorescence units). No significant
260 emission below 400 nm or above 650 nm is observed. C) Photographs of 2 fields of view of
261 unstained 10 μm thick brain section of grey matter in a case of FTLT-T imaged at Alexa 488 (λ_{ex}
262 = 488 nm, λ_{em} = 493-570 nm) and Texas Red (λ_{ex} = 561 nm, λ_{em} = 601-635 nm) channels 0 to 72
263 hours after photobleaching. Distinct fluorescent particles resembling lipofuscin are observed and
264 their signal intensities are reduced after 72 hours of photobleaching, although a few dim
265 fluorescent bodies remain. Scale bar = 100 μm .

266 **Figure 2: Quantification of LED-induced signal intensity reduction of lipofuscin**
267 **fluorescence in two fields of view.** Each dot represents the signal intensity of one lipofuscin
268 particle present in a field of view at Alexa 488 (left) and Texas Red (middle) channels. Particles
269 from two 425 $\mu\text{m} \times 425 \mu\text{m}$ fields of view are quantified and plotted. The population of
270 fluorescent particles shifts to reduced intensity levels after photobleaching. The mean and
271 standard deviation of the population is plotted (right) and fitted to the exponential decay function
272 $y = y_0 + Ae^{\frac{-x}{T}}$, where y is the intensity, y_0 is the baseline intensity, A is the initial maximum
273 intensity, x is the photobleaching duration, and T is the decay constant. The fitted parameters for
274 each channel is listed under their figure legends.

Figure 3: Immunofluorescence imaging of phospho-tau stained FTLD-T formalin-fixed brain tissue. 10 μm thick sections were stained with AT8 primary antibody and Texas Red and Alexa 488 conjugated secondary antibodies. Slides were counterstained with DAPI. The signals from Alexa 488 ($\lambda_{\text{ex}} = 488 \text{ nm}$, $\lambda_{\text{em}} = 493\text{-}570 \text{ nm}$), Texas Red ($\lambda_{\text{ex}} = 561 \text{ nm}$, $\lambda_{\text{em}} = 601\text{-}635 \text{ nm}$), DAPI ($\lambda_{\text{ex}} = 405 \text{ nm}$, $\lambda_{\text{em}} = 410\text{-}507 \text{ nm}$) and a merged image are displayed. Multiple autofluorescence reduction methods including 48 hour photobleaching, TrueBlack™, Eriochrome Black T, and non-treatment are tested. Signal profiles at the cross section indicated by the dotted lines on the merged panels are quantified. Signal peaks representing Tau inclusions (T), nuclei (N) or lipofuscin particles (L) are labeled. Scale bar = 100 μm .

Figure 4: Immunofluorescence imaging of phospho-tau and Nissl stained FTLD-T formalin fixed brain tissue using photobleaching and TrueBlack™ treatments. 10 μm thick sections were stained with AT8 primary antibody and Alexa 488 conjugated secondary antibody, NeuroTrace® fluorescent Nissl stain, and DAPI. The signals from Alexa 488 ($\lambda_{\text{ex}} = 488 \text{ nm}$, $\lambda_{\text{em}} = 493\text{-}570 \text{ nm}$), Nissl ($\lambda_{\text{ex}} = 561 \text{ nm}$, $\lambda_{\text{em}} = 601\text{-}635 \text{ nm}$), DAPI ($\lambda_{\text{ex}} = 405 \text{ nm}$, $\lambda_{\text{em}} = 410\text{-}507 \text{ nm}$) and a composite channel are displayed. The sections are either photobleached prior to staining, or treated with TrueBlack™ after staining. Scale bar = 100 μm .

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